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The intensive care patient population is changing. Increasingly intensive care units (ICUs) are treating older patients, with more comorbidities, and variable prognosis, at a time when family expectations are different and often with higher expectations of recovery. Life support technology is increasingly sophisticated, surgery is minimally invasive in many cases and nonsurgical interventions such as interventional radiology have come to play a greater role in patient care.

The intensive care unit has benefited greatly from advances in imaging—from diagnosis to planning and monitoring treatment. The radiology-ICU partnership is still evolving, building on recent advances in functional imaging.

Medical specialties by their very nature can work in semi-isolation. While both radiology/imaging and intensive care medicine have become more specialised, they both have more horizontal cross-collaborative practices. Communication is more challenging because of increasing complexity, e.g. determining the significance of T2 weighting on a brain magnetic resonance imaging (MRI) scan, or an unstable patient with invasive haemodynamic monitoring in situ requiring cerebral angiography. The acute nature of work is more accentuated, e.g. uncontrollable gastrointestinal (GI) bleed, the need for a computed tomography (CT) scan of the brain prior to thrombolytic therapy, and deciding where the patient goes to after the procedure.

Challenges for the intensive care doctor include keeping up-to-date with advances in all modes of imaging (CT, angiography, MRI, positron emission tomography [PET], ultrasound). Clear communication with the imaging department about the need and potential benefit from an imaging procedure is essential, as is knowing when and where to apply a particular imaging technique to an individual patient. The financial perspective should always be recognised by the intensivist requesting an imaging procedure. Point-of-care ultrasound enables many examinations to be done at the bedside. Logistical challenges remain when transporting mechanically ventilated patients to the imaging department. Translation of findings into everyday clinical practice can also be challenging.

Medical imaging provides structural information, functional imaging and real-time imaging of tissue metabolic activity (Figure 1).

**Neuroimaging**

*Magnetic resonance imaging*

MRI has great value in the ICU for prognostication. A recent systematic review and meta-analysis of studies evaluating the predictive value of acute MRI lesion patterns for discriminating clinical outcome in traumatic brain injury confirmed that MRI following traumatic brain injury yields basic anatomical abnormalities.

**Basic anatomical abnormalities**

e.g. CXR, CTB, US

![Diagram of imaging modalities](image)

**Tissue characterisation**

MRI, PET

**Tissue perfusion**

MRI, CT, Contrast US

**Tissue metabolic activity**

PET, MRI

? Future

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**Figure 1.**

CXR chest x-ray CT computed tomography CTB computed tomography brain MRI magnetic resonance imaging PET positron emission tomography US ultrasound

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important prognostic information (Haghbayan et al. 2017). Already, functional MRI can compare activation patterns in the brain with task functional MRI (fMRI) mapping with subjects performing a simple ‘hand task’ (Ugurbil 2016).

CT scanning
CT brain scanning is usually readily available for the critically ill patient due to organisational preferences in imaging departments. CT scanning has developed to provide advanced structural and functional tissue characterisation. Increasingly used to triage stroke patients, CT perfusion imaging distinguishes normal from abnormal perfusion. It can identify an ischaemic penumbra for example. It is more sensitive for detecting cerebral contusions. Perfusion neuroimaging techniques include CT bolus perfusion, MR imaging bolus perfusion, MR arterial spin labeling perfusion and xenon CT, as recently explained by Douglas et al. (2018).

In acute traumatic brain injury, contrast-enhanced perfusion CT, as illustrated by Lui et al. (2010), can be used to differentiate salvageable tissue from unsalvageable tissue (Figure 2, Figure 3).

Functional brain scanning
The brain represents 2% body weight, and uses 15% cardiac output, 20% total body O₂ consumption and 25% total body glucose consumption (Villien et al. 2014). MRI and PET are suitable for structural brain imaging, but not yet suitable for functional brain scanning, as explained below.

The radiotracer 18 F-fluorodeoxyglucose (FDG) has been used to study brain glucose metabolism by PET for the past 40 years. However the “snapshot” takes 20-40 minutes post bolus and it is difficult to obtain temporal resolution compared to fMRI. A recent
technique (fPET-FDG) that uses constant infusion FDG appears promising (Villien et al. 2014).

fMRI has good temporal resolution, which is obtained in one pass. Blood oxygen-level dependant (BOLD) is widely employed for brain mapping. However, it is not quantitative in the absolute sense.

Cardiac imaging
Cardiac MRI and myocardial injury
Cardiac MRI can show myocardial tissue structure in detail using the contrast agent gadolinium. Gadolinium differentially accumulates in regional segregated tissue such as a post-infarction scar, thus known as late gadolinium enhancement (LGE) (Puntmann et al. 2016). However, it is not so helpful where diffuse disease is present, as a continuum of disease is present with no reference in the imaging plane. Gadolinium shortens T1 time and the difference

Table 1. Time related parameters in MRI scanning

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Normal</th>
<th>High/longer – fibrosis/inflammation/oedema</th>
</tr>
</thead>
<tbody>
<tr>
<td>T1 pulse sequence</td>
<td></td>
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<tr>
<td>T1 - Time taken for correction to underlying magnetic plane following administration of a radiofrequency (RF) pulse. (e.g. 180°)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>T1 faster - Fe, fat</td>
<td>Normal</td>
<td>High/longer – fibrosis/inflammation/oedema</td>
</tr>
<tr>
<td>T2 pulse sequence</td>
<td></td>
<td></td>
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<tr>
<td>T2 is the time taken to return to normal following RF pulse causing rotational move, i.e. precision factor normally T2&lt; T1</td>
<td></td>
<td></td>
</tr>
<tr>
<td>T2 high/longer - inflammation oedema</td>
<td></td>
<td>i.e. if only T1 is high/longer then there is likely to be underlying fibrosis</td>
</tr>
</tbody>
</table>

$ECV = \left(1 - \text{haematocrit}\right) \frac{1}{\text{post contrast T1 myo}} - \frac{1}{\text{native T1 myo}} \frac{1}{\text{post contrast T1 blood}} - \frac{1}{\text{native T1 blood}}$

Source: Haaf et al. (2016) Reproduced under CC BY 4.0 (creativecommons.org/licenses/by/4.0)

Cardiac MRI can show myocardial tissue structure in detail using the contrast agent gadolinium. Gadolinium differentially accumulates in regional segregated tissue such as a post-infarction scar, thus known as late gadolinium enhancement (LGE) (Puntmann et al. 2016). However, it is not so helpful where diffuse disease is present, as a continuum of disease is present with no reference in the imaging plane. Gadolinium shortens T1 time and the difference

Figure 4. T1 mapping and ECV in clinical practice

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Tissue characterisation using native T1 and extracellular volume fraction (ECV). Absolute values for native T1 depend greatly on field strength (1.5 T or 3 T), pulse sequence (MOLLI or ShMOLLI), scanner manufacturer and rules of measurements. For the purpose of comparability, only studies using 1.5 T scanners were considered in this figure.

Figure 5

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Cardiac imaging
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Cardiac MRI can show myocardial tissue structure in detail using the contrast agent gadolinium. Gadolinium differentially accumulates in regional segregated tissue such as a post-infarction scar, thus known as late gadolinium enhancement (LGE) (Puntmann et al. 2016). However, it is not so helpful where diffuse disease is present, as a continuum of disease is present with no reference in the imaging plane. Gadolinium shortens T1 time and the difference

Figure 6.

Source: Driessen et al. (2017) Reproduced under CC BY 4.0 (creativecommons.org/licenses/by/4.0)
between T1 native and T1 gadolinium gives an idea of how much gadolinium is in the extracellular myocardium providing a guide to extracellular volume.

Diffuse myocardial processes can be shown with cardiac MRI, including inflammation, oedema, extravascular volume expansion, infiltrative disease, microvascular ischaemia and fibrosis.

**Myocardial oedema**
Laine and Allen in 1991 demonstrated in a study of dogs implanted with porous polyethylene capsules that measured end-diastolic interstitial fluid pressure in the left ventricle, that acute myocardial oedema compromises cardiac function and that chronic right heart pressure elevation and chronic arterial hypertension produce left ventricular myocardial oedema (Laine and Allen 1991).

Now pulsing MRI techniques can be used to assess myocardial oedema. On MRI it shows as increased global left ventricular T2 values that decrease with successful decongestion (Verbrugge et al. 2017).

**Native T1 (T1 imaging without contrast)**
T1 time measures the time taken to recover longitudinal magnetisation. It is moderately water sensitive and elevated in diffuse myocardial fibrosis, inflammation and oedema (Taylor et al. 2016).

**Imaging extracellular volume fraction (ECV)**
MRI can be used to image myocardial extracellular volume fraction (Figure 4). The process first obtains T1 in myocardium and blood precontrast, then after administration of gadolinium obtains T1 in the myocardium and blood. ECV is elevated in expansion of extracellular space such as amyloid and myocardial oedema. Imaging can quantify ECV and confirm expansion of extracellular space. The measures are pre- and post-contrast T1 relaxation times of blood and myocardium with correction for blood volume of distribution via the haematocrit (Figure 5).

For ICU patients native T1 MRI imaging can be used to assess inflammation, myocardial oedema and expansion of extracellular volume fraction as well as microvascular dysfunction/microvascular ischaemia.

**Myocardial perfusion using PET**
Hybrid PET/CT scanners can provide anatomical and functional information, as shown in Figure 6. This shows a 46-year-old male with typical anginal chest pain. The PET scan shows an inferolateral perfusion defect with a myocardial flow reserve 1.75. Coronary computed tomography angiography (CCTA) showed an obtuse marginal defect. Fused PET and CCTA showed a downstream perfusion defect. Invasive coronary angiography showed marked luminal obstruction with a fractional flow reserve (FFR) of 0.34.

**Conclusion**
Intensivists need to be proactive: find out what technology is available in their institution.

**Case studies**
Two illustrative case studies are on the next pages.

**Conflict of interest**
Anthony McLean declares that he has no conflict of interest.

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**Abbreviations**
- ACA anterior cerebral artery
- CBV cerebral blood volume
- CCTA computed tomography
- CBV cerebral blood volume
- CIA internal carotid artery
- ICA internal carotid artery
- ICU intensive care unit
- MCA middle cerebral artery
- MIT mean transit time
- PCA posterior cerebral artery
- PET positron emission tomography
- PET positron emission tomography
- T1 mapping: basic techniques and clinical applications. JACC Cardiovasc Imaging, 18(7):787-794.

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**References**


Case 1

26-year-old woman, G2 P1 in her 2nd uncomplicated pregnancy
Presented at 34 weeks – hypertension, headache, visual changes
Reflexes not increased
Urinary protein +++
Prescribed Magnesium sulfate (MgSO4), hydralazine
Fetal distress, went for caesarean section
Admitted to ICU post delivery (late afternoon)
Blood pressure (BP) well controlled, comfortable
Nil headache or visual changes
Brisk reflexes, ankle – 1 beat of clonus
Stat dose clonidine given overnight BP 150/83

0600 next morning unresponsive, incomprehensible noises
Normal reflexes, BP 171/99
No focal neurological defects on examination

Image 1 shows the CT scan of the brain showed no dural vein thrombosis.

Image 2 shows early ischaemic change in both cerebellar hemispheres on fluid-attenuated inversion recovery (FLAIR) MRI (no concurrent diffusion change).

Image 3 shows extensive restricted diffusion within grey and white matter consistent with ischaemia in the frontal lobes, left parietal lobe, and to a lesser extent in the right parietal lobe.

Image 4 is the 3D time-of-flight imaging, which shows a smooth tapered narrowing of basilar artery and generalised narrowing of anterior circulation arteries bilaterally, suggestive of vasospasm.

The pathophysiology in this case suggested differential diagnosis of eclampsia-induced vasospasm, eclampsia-associated Posterior Reversible Encephalopathy Syndrome (PRES), eclampsia-associated Reversible Cerebral Vasconstriction Syndrome (RCVS) or eclampsia-associated RCVS-PRES overlap.

The final diagnosis was eclampsia-associated RCVS-PRES overlap.
Case 2

41-year-old woman, history of hypertension/diabetes II
Argument with brother – loud and angry, followed by sudden collapse
No striking of head, no obvious seizure
Stopped breathing for 2 minutes
CPR by family 10-15 minutes
Ambulance arrived - patient had underlying cardiac rhythm, applied automated external defibrillator (AED)
ED - decerebrate posturing, intubated, urgent CTB
CTB (Image 5) - no bleed, subtle hypodensity in right basal ganglia and anterior temporal lobe associated with mild effacement of overlying sulci.
Diagnosis: possible early infarction

CT angiography (image 7) – no filling defect to suggest acute thrombus
Bilateral ACA/ MCA/ PCA normal
Large left PCA/ absent right PCA
Basilar artery supplied by large left vertebral artery
Right vertebral artery small vessel which directly supplies the posterior inferior cerebellar artery

Image 7 Cerebral CT perfusion scan totally normal
CBV cerebral brain volume MTT mean transit time TTP time to peak

Patient outcome: no neurological deficits, ‘normal on discharge’